Dentistry Section

Effect of Four Surface Treatment Methods on the Shear Bond Strength of Resin Cement to Zirconia Ceramics- A Comparative in Vitro Study

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ABSTRACT

Background: Improving the retention of zirconia-based ceramics is desirable in order to avoid the failure of crowns and fixed partial dentures .This can be achieved by creating micromechanical retention using surface treatments. Therefore, it becomes necessary to constantly compare and re-evaluate the influence of different surface treatment methods on the bond strength .

Aim: To evaluate the effect of four different surface treatments on shear bond strength between zirconia surface and resin cements.

Settings and Design: Observational study.

Materials and Methods: Twenty five zirconia plate samples were prepared based on ISO standards and were divided into five groups and each group was subjected to following five different surface treatments : no treatment, sandblasting with 110 µm

alumina, sandblasting with 250 µm alumina, acid etching with 9.6% hydrofluoric acid and laser radiation on the surface. All the samples were surface disinfected and were embedded in blocks of autopolymerising resin to check shear bond strength on the universal testing machine. Statistical analysis used-data was analyzed using one-way ANOVA and a Post Hoc Bonferroni test.

Results: Analysis of the data showed that the highest shear bond strength values were obtained with laser treatment (18.120 \pm 0.8159 Mpa). The lowest values were obtained with control group (9.166 \pm 0.569 Mpa). Laser treatment increased the shear bond strength values significantly (p<0.05).

Conclusion: Surface treatments increased the bond strength between zirconia and resin cement and carbon dioxide laser could be an effective surface treatment for increasing bond strength.

Keywords: Airborne particle abrasion, Carbon dioxide laser, Hf acid etching, Laser etching, Shear bond strength, Surface treatment

INTRODUCTION

Success of an all ceramic restorations is highly dependent on achieving a bond of the resin with the underlying tooth structure as well as with the restoration. Bonding is required for improving the retention, marginal adaptation, fracture resistance and bond strength of restorations [1]. Bonding also increases surface energy, surface area for bonding, and wettability [2]. During the fabrication or milling of the ceramic, sufficient bond strength values are not generated, therefore it requires surface pretreatment [3]. Bond strength can be improved by the presence of micromechanical retention, as the creation of roughened ceramic surfaces may allow resin cement to penetrate and flow into such microretentions, thereby creating a stronger micromechanical interlock [4]. There are several tests for assessment of bond strength of resin-based materials to dental ceramics namely shear, tensile, and microtensile tests. These test methods are based on the application of a load in order to generate stress at the adhesive joints until failure occurs [5].

There are various surface treatment methods namely grinding, abrasion with diamond rotary instruments, airborne particle abrasion, silicate coating, acid etching, coupling with silane and combinations of any of these methods [4,5]. Airborne particle abrasion with aluminium oxide abrasive particles has been identified as an effective means of achieving a stable, durable bond for zirconia ceramics [6]. Acid etching on a zirconia ceramic surface has been found to produce a significant difference in the surface roughness [4]. A few studies have also been performed on the carbon dioxide laser treatment of zirconium oxide ceramics [5,7].

Considering the various materials and techniques available, influence of surface treatment on bond strength with commonly available

modalities like sandblasting, acid etching, and laser treatment was planned. So the first NULL hypothesis for the present study was that the type of surface treatment does not significantly affect the shear bond strength of zirconia to tooth structure .The second NULL hypothesis was that the carbon di oxide laser does not have a determinant effect and could not be an effective surface treatment modality to increase bond strength.

MATERIALS AND METHODS

Twenty five samples of zirconia, CEREC (Cortis-YZ, Sirona Dental GmbH Bensheim, Germany) were sliced off from the blocks using the diamond disc under running water and assorted into groups and sintered for 8 hours [Table/Fig-1] following manufacturer's instructions(www.sirona.com/en/products/digital-dentistry/ newproducts/information). Then the samples were trimmed and prepared to size of 16 x 11 mm uniformly following ISO -682, 2008 guidelines [8] for sample preparation. All the samples were then surface disinfected with isopropyl alcohol (Surfacept, Minntech Corporation Minneapolis, USA), smoothened with emery paper under running water and then cleaned in ultrasonic cleanser.

Subsequently the samples are divided into five Groups, Group A samples were left untreated and served as control group for the study. Group B samples were sandblasted with 110 μ m alumina (KoroxR110 microns Bego, Bremen, Germany) at 35 psi from a distance of approximately 10mm for 15 secs. Group C samples were sandblasted with 250 μ m alumina (KoroxR110 microns Bego, Bremen, Germany) at 35 psi from a distance of approximately 10mm for 15 seconds. Group D samples were acid etched with 9.6% hydrofluoric acid (Ultradent porcelain etch 9.6%, Ultradent Products,



[Table/Fig-1]: Sintering

[Table/Fig-2]: Universal testing machine

Group	Treatment	Mean	SD			
А	Control	9.1660	.56968			
В	Sand blasting 110 mm silica	10.890	.85591			
С	Sand blasting 250 mm silica	10.732	1.17238			
D	HF acid treatment	12.6060	.53069			
E	LASER treatment	18.120	.8159			
SD – Standard Deviation						

[Table/Fig-4]: Mean and Standard Deviation of shear bond strength of Control and Experimental Groups

South Jordan) for 30 sec and then air dried. Group E samples were treated with surgical carbon dioxide laser radiation (Smart US 20D, Carbon Dioxide laser, Deka Floresence, Italy) on the surface. Laser energy was delivered in a pulse mode with wavelength of 10.6 mm, a pulse repetition rate of 1000 Hertz and pulse duration of 160 ms at an average power setting of 3 w, delivered perpendicular to the surface in non-contact mode 1mm away from the surface.

All the samples were once again surface disinfected with isopropyl alcohol to remove off debris and were embedded in blocks of autopolymerising resin to facilitate clamping on the universal testing machine (Mechanical Krystal Elmec, Ichkalkaranji, Maharashtra, India) [Table/Fig-2]. Resin cement blocks of 0.5 mm were embedded over treated surface using LEDition (LED lamp LUX-V Guilin woodpecker medical instrumentation co.Guangxi, China) with Intensity of 600- 800W/cm2 for 20 sec following manufacturer's instructions. The samples were loaded in the universal testing machine and pulled apart after clamping in the opposite jaws [Table/Fig-2,3] to find the shear bond strength. A thin wire of 0.2 mm diameter was looped around and a shear force was applied at cross head speed of 1mm/minute. The shear bond strength was calculated in Megapascal by dividing Failure load (N) by area of composite resin (mr2). Results obtained were tabulated and subjected for statistical analysis. Means and standard deviations of the bond strength were calculated and mean values were compared by one-way ANOVA using Statistical software program, Statistical Package for the Social Sciences (SPSS, Version 19; IBM SPSS Inc., Chicago, Illinois). Multiple comparisons test were done using Bonferroni post hoc test.

RESULTS

[Table/Fig-4] yielded the highest shear bond strength values for lasers(18.120 \pm 0.8159 Mpa) and lowest values were obtained for control group (9.166 \pm 0.569 Mpa) [Table/Fig-4].One-way ANNOVA [Table/Fig-5] yielded p-value <0.05 which shows that the results were significant [Table/Fig-5]. There were no significant differences in p-value between control, sandblasting with 110 μ m and sandblasting with 250 μ m. Laser showed significant differences from all other groups (p < 0.05). On analysis of Bonferroni post hoc test results [Table/Fig-6], it was found that on comparing other groups with control, both HF and laser groups had better bond



[Table/Fig-3]: Samples clamped in the UTM

	Sum of squres	Df	Mean square	F	Р			
Groups		4						
Within groups	13.68	20	69.238	101.18	.000			
Total	290.63	24	.684					
[Table/Fig-5]: Results of one- way ANOVA test., P<0.05 indicates statistically significant differences. Df – degrees of freedom, F-F statistic, p- statistical significance								

strength. When both air abrasion group was compared with other groups only laser treatment group had statistically significant values. HF group when compared with other groups was found to be better similar to control group. Finally, when laser group was compared with the rest it was found to have statistically significant values than any other group.

DISCUSSION

The data in the present study rejected the first null hypothesis, as the bond strength between zirconia and resin cement was affected by the type of surface treatment similar to some previous studies [9]. The present study also rejected the second null hypothesis and carbon di oxide laser was found to improve the shear bond strength between zirconia and tooth structure. Several tests can be used for assessing bond strength namely, shear, tensile and microtensile tests. Tension tests are more appropriate for assessing adhesive characteristics of the resin cements to the ceramics which is not applicable in the present situation since our study aimed to determine the effect of surface pretreatments on bond strength. Microtensile test was not appropriate for the present study because multiple specimens from the same block leads to difficulties in statistical interpretation of the results. In the present study, shear bond has been used for comparison, as it is commonly used, is fast, easy to perform and also reflects the clinical situation [3]. There was no significant difference in the shear bond strength between the control, sandblasting and acid etching groups except in the laser group [Table/Fig-7].

Some studies have shown that some conventional and selfadhesive resin cements presented low bond strength when applied to intact surfaces of Zirconium oxide ceramics [10]. Improving the retention of zirconia-based ceramics is desirable in order to avoid the decementation phenomena [11,12]. Loss of crown retention was found to be the second leading cause of failure of crowns and fixed partial dentures [13]. Uncemented restorations have been listed as the third leading cause of prosthetic replacement with failures occurring in varying periods of 1 to 38 month [11,12] and 5.8 y of service [14]. Failures are usually reported as being within the substrate(cohesive),between the adhesive and substrate(adhesive),within the restorative material (cohesive),or mixed.

Air abrasion was proposed in order to increase the resin bond strength to zirconia [15] and the cement to ceramic bonding [16]. However it was found that particle abrasion alone, slightly roughens

(I) Distribution of Group	(J) Distribution of Group	Mean Difference (I-J)	Std. Error	Р
Control	Sand blasting with 110 mm silica	-1.72800*	.52318	.036
	Sand blasting with 250 mm silica	-1.56600	.52318	.072
	Hydrofluoric acid	-3.44000*	.52318	<0.001
	CO ₂ laser treatment	-9.54600*	.52318	<0.001
Sand blasting	Control	1.72800*	.52318	.036
with 110 mm silica	Sand blasting with 250 mm silica	.16200	.52318	1.000
	Hydrofluoric acid	-1.71200*	.52318	.038
	CO ₂ laser treatment	-7.81800*	.52318	<0.001
Sand blasting	Control	1.56600	.52318	.072
with 250 mm silica	Sand blasting with 110 mm silica	16200	.52318	1.000
	Hydrofluoric acid	-1.87400*	.52318	.019
	CO ₂ laser treatment	-7.98000*	.52318	<0.001
Hydrofluoric	Control	3.44000*	.52318	.000
acid	Sand blasting with 110 mm silica	1.71200*	.52318	.038
	Sand blasting with 250 mm silica	1.87400*	.52318	.019
	CO ₂ laser treatment	-6.10600*	.52318	<0.001
CO ₂ laser	Control	9.54600*	.52318	<0.001
treatment	Sand blasting with 110 mm silica	7.81800*	.52318	<0.001
	Sand blasting with 250 mm silica	7.98000*	.52318	<0.001
	Hydrofluoric acid	6.10600*	.52318	<0.001

*. The mean difference is significant at the 0.05 level., P- statistical significance



the zirconia surface [17] but does not always provide reliable resin bond strength [2,15]. Different sizes of aluminium oxide particles, between 50 and 110 mm, are generally used for sandblasting [15]. However, it was found that different size of particles and the application time may induce discrepancies in the achieved results, as excessively high pressure during blasting may initiate phase transition, and expedite the formation of micro-cracks, thus reducing the mechanical properties of zirconia [18]. In the present study particle size of alumina did not show any difference (p>0.05).

Acid etching on a zirconia ceramic surface produced a significant difference in the surface roughness [4]. Contrary to it was also found that etching with hydrofluoric acid has no influence on zirconia ceramics, as no micro-grooves are created, due to the low amount of glass phase [19,20], and its susceptibility to hydrolytic degradation [15,21]. However, the present study showed better effectiveness of HF group similar to Ural et al., [22].

Carbon dioxide lasers have been previously used to etch zirconia bioceramic implants to enhance their osseointegration [23] and improve adhesion of orthodontic metal brackets to feldspathic porcelain. It has been reported that carbon di oxide laser etching produces a lower bond strength when compared with chemical etching [24] and is less effective for improving Zirconia bonding as compared to other lasers [25-27]. Although, there have been

negative results for lasers, but in some studies [22] carbon di oxide laser enhanced micromechanical retention and improved the bond strength of resin cement on zirconia ceramic when compared with other surface treatments similar to our study.

An effective bonding between the tooth structure and zirconia would prevent the removal of more tooth structure to create retention and resistance form for the restoration. In addition, it would aid in retention of teeth with short or reduced clinical crowns [28]. However, clinically there are many other factors which lead to the dislodgement of crown. In the present study surface analysis tests using scanning electron microscopy, or x-ray diffraction method were not done which may be considered as a limitation of the study. Our aim however was to determine the bond strength in this study and not to assess the surface characteristics.

CONCLUSION

Within the limitations of the present study, it was possible to conclude that the surface treatments increased the bond strength and the type of surface treatment significantly affected the shear bond strength of zirconia to tooth structure. Carbon dioxide laser proved to increase bond strength. A chairside system of carbon di oxide laser may be effective in improving the shear bond strength between a zirconia ceramic and tooth structure.

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